

Ultra-wide-angle Wireless Endoscope with a Backend-camera-controller Architecture

Dongha Shim and Jason Yi

Abstract—This paper presents a wireless endoscope with an ultra-wide FOV (Field of View) of 130° and HD resolution (1280x720 pixels). The proposed endoscope consists of a camera head, cable, camera controller, and wireless handle. The lens module with a 150° degrees AOV (Angle of View) is achieved using the plastic injection-molding process to reduce manufacturing costs. A serial CMOS image sensor using the MIPI (Mobile Industry Processor Interface) CSI-2 (Camera Serial Interface-2) interface physically separates the camera processor from the camera head. The camera head and the cable have a compact structure due to the BCC (Backend-Camera-Controller) architecture. The size of the camera head and the camera controller is 8x8x26 mm and 7x55 mm, respectively. The wireless handle supports a UWB (Ultra-Wide-Band) or a Wi-Fi communication to transmit video data. The UWB link supports a maximum data transfer rate of ~ 37 Mbps to transmit video data with a resolution of 1280x720 pixels at a frame rate of 30 fps in the MJPEG (Motion JPEG) format. Although the Wi-Fi link provides a lower data transfer rate (~ 8 Mbps Max.), it has the advantage of flexible interoperability with various mobile devices. The latency of the UWB link is measured to be ~ 0.1 sec. The Wi-Fi link has a larger latency (~ 0.5 sec) due to its lower data transfer rate. The proposed endoscope demonstrates the feasibility of a high-performance yet low-cost wireless endoscope using the BCC architecture. To the best of the author's knowledge, the proposed endoscope has the largest FOV among all presently existing wireless endoscopes.

Keywords—Wireless endoscope, ultra-wide-angle, plastic lens, backend-camera-controller, serial image sensor, ultra-wide-band, Wi-Fi, latency

I. INTRODUCTION

AN endoscope has always been an indispensable tool for various medical and industrial applications. Medical endoscopy has evolved into various types (e.g., gastroscopy, colonoscopy, bronchoscopy, rhinoscopy, otoscopy, and capsule) depending on specific diagnoses and treatments [1]-[5]. Industrial endoscopes are extensively employed in non-destructive visual inspections of various parts in the aircraft, automobile, and plant industry, including engines, pipes, and turbines [6]. Other applications can be also found in security, rescue, and police/military operations. Recently, low-cost endoscopes are being widely deployed. In particular, a wireless endoscope has become increasingly more popular due to its convenience in use and the significant reduction in its cost [7]-[11]. Most commercial wireless endoscopes have a limited

FOV (Field of View) of 60° or less, and they do not have a bending distal tip because of cost limitations. The proposed endoscope employs an ultra-wide-angle lens module to resolve the issue. All lenses in the lens module are injection-molded to reduce the manufacturing costs.

Most low-cost commercial wireless endoscopes employ a parallel CMOS image sensor and a Wi-Fi communication link [7]-[11]. Few of them support the resolution levels above VGA (640x480 pixels), as their configurations have some limitations in supporting a higher video resolution. A parallel sensor with a higher resolution requires interconnections that are more complicated and thereby increases the size of the camera head. In addition, the larger number of connections is responsible for its relatively large power consumption, which is a crucial weakness for battery-powered mobile applications. The Wi-Fi communication link often cannot provide the required data transfer rate for a higher video resolution (above VGA) due to its limited bandwidth. Therefore, commercial Wi-Fi endoscopes often experience a noticeable delay similar to that faced by Wi-Fi cameras due to their low data transfer rates [12]. A new architecture for a wireless endoscope needs to be developed to support higher quality video with a high-speed data transmission capability.

In commercial wireless endoscopes, a camera controller is usually packaged in a camera head along with a parallel image sensor to keep the interconnections short. The camera controller processes the image data and communicates to a terminal device using a generic protocol (e.g., USB). The size and complexity of the camera head can be significantly reduced if it included only the image sensor physically separated from the camera processor. The proposed endoscope employs a low-cost commercial serial image sensor with a MIPI (Mobile Industry Processor Interface) CSI-2 (Camera Serial Interface-2) interface [13]. A flexible cable placed between the image sensor and the camera processor achieves the BCC (Backend-Camera-Controller) architecture [14]. A serial image sensor consumes less power than a parallel one, thereby extending the battery-operation-time of a wireless endoscope. The proposed endoscope employs a high-speed UWB (Ultra-Wide-Band) for the communication link. The wide bandwidth of the UWB link allows transmissions of high-resolution video at a high data transfer rate. The wireless endoscope also supports a Wi-Fi link to take advantage of its flexible interoperability with various mobile devices. A prototype of a high-performance wireless endoscope is implemented using the BCC architecture and the high-speed UWB link. Measurements evaluate the optical, video and latency characteristics of the prototype endoscope.

This work was supported by the Research Program funded by the SeoulTech (Seoul National University of Science & Technology), Korea.

D. Shim is with SeoulTech (Seoul National University of Science & Technology), Seoul, Korea (e-mail: dongha@seoultech.ac.kr).

J. Yi is with Haesung Optics Co., Ltd., Suwon, Korea (e-mail: jsyi@hso.co.kr).

II. ARCHITECTURE OF WIRELESS ENDOSCOPE

For obvious reasons, a long cable should be avoided while interconnecting a parallel image sensor and a camera processor. First, a long interconnecting cable would introduce a synchronization issue among parallel data and clock channels [15]. Second, multiple parallel data lanes required by the image sensor would make the cable between a parallel image sensor and a camera processor bulky and stiff, limiting the accessibility and maneuverability of the endoscope [15]. Third, the increased complexity of the camera head and the long interconnecting cable would result in additional manufacturing costs. A parallel image sensor with a higher resolution needs more interconnections, which is a major bottleneck in achieving a high resolution endoscope.

The above issues can be resolved by using an image sensor with a serial interface using less interconnection for data lanes. The MIPI CSI-2 standard features a serial, fast, and low-power interface between a peripheral image module and a mobile device, ensuring relatively small dimensions [13].

Fig. 1 shows the structure of the proposed wireless endoscope with the BCC architecture using the MIPI CSI-2 image sensor. The endoscope consists of the camera head, a cable, a camera controller, and a wireless handle. The image sensor in the camera head connects to the camera controller through a multi-strand flexible cable. The camera controller converts the MIPI-enabled serialized digital sensor output into a UVC (USB Video Class) format, and directly communicates the UVC digital video to the wireless handle via a USB 2.0 cable. The wireless handle transmits the video data to a terminal device by either the UWB or the Wi-Fi communication link depending on the selected mode.

Fig. 2 shows the photo of the implemented wireless endoscope prototype. A wireless endoscope with a higher resolution can be achieved using the proposed BCC architecture along with the high-speed UWB link.

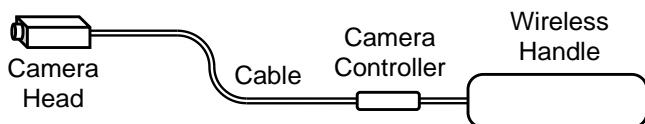


Fig. 1. Configuration of the ultra-wide-angle wireless endoscope with the backend-camera-controller configuration.

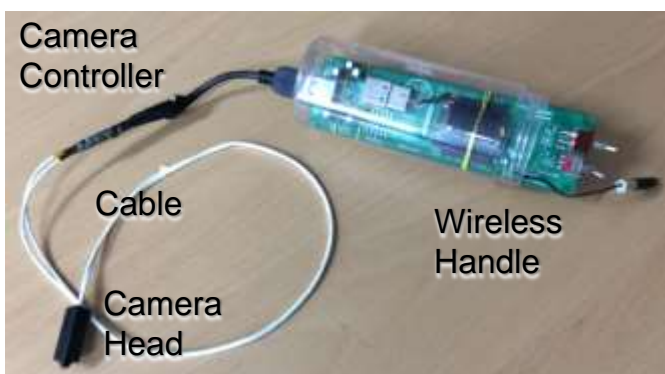


Fig. 2. Photo of the proposed wireless endoscope prototype.

III. IMPLEMENTATION OF WIRELESS ENDOSCOPE

A. Camera Head

Fig. 3 shows a 3-D exploded view of the camera head. It consists of a lens module, a holder, an image sensor, an interface board, and a case. Four aspheric lenses implement the ultra-wide-angle lens module with a 150° AOV (Angle of View) [16]. To reduce the manufacturing costs, all lenses are injection-molded using PMMA (Polymethyl Methacrylate) and no glass lenses are used. The AOV of the lens module is estimated to be $\sim 150^\circ$ with an F-number of 3.5, and an EFL (Effective Focal Length) of 1.02 mm. The lens module has the diameter and length of 3.5 and 3.1 mm, respectively [16].

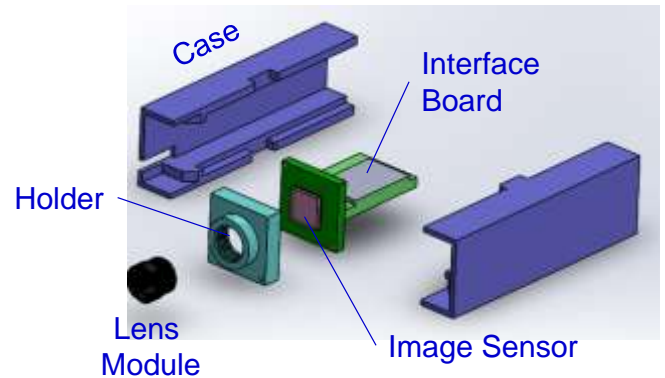


Fig. 3. 3-D exploded view of the proposed camera head.

A commercial CMOS color image sensor reduces the size and cost of the camera module [17]. The image sensor uses the CSI-2 interface of the MIPI standard, which is widely adopted by conventional mobile devices. The MIPI standard features high performance to support a high data rate at low power consumption [13]. The image sensor has a one-lane high-speed CSI-2 serial data interface that reduces the number of interconnections significantly compared to those of a parallel image sensor [17]. It supports the high-definition resolution of 1280×720 pixels (720p) at a frame rate of 30 fps. The package size of the image sensor is 3.8×3.3 mm with a pixel size of 1.75×1.75 μm . Its low-power characteristic is especially critical for a mobile device powered by a battery. A parallel image sensor with similar specifications consumes 3x higher power [18]. The image sensor is mounted on a 7×7 mm PCB soldered perpendicular to the interface board. The interface board has a compact size of 7×11 mm, and does not include any other electronic component. The interface board connects to the camera controller through a ~ 70 -cm long flexible cable containing multiple strands. The 14-strand cable offers interconnections for the MIPI data/clock lanes, the serial camera control bus, the system clock, the power supplies, and grounds. Although the cable has 24 strands, only 14 are used as the cable was chosen based on easy availability.

The camera unit is packaged within a plastic case. Fig. 4 shows a photo of the packaged camera head. The size of the camera module is $8 \times 8 \times 26$ mm. The inset in the figure shows an illumination unit mounted on the holder. The unit has two white small-footprint chip LEDs with a size of 1.6×0.8 mm each. The camera head can be further reduced using a smaller image sensor with more compact design [16].



Fig. 4. Photo of the manufactured camera head. The inset show the illumination unit mounted on the holder.

B. Camera Controller

Fig. 5 shows the top and the bottom side of the camera controller. A camera processor processes the video data and communicates with the wireless handle via the UVC interface [19]. The unit can transfer videos up to FHD (1920x1080 pixels) at 30 fps, streaming in the uncompressed YUY2 or the MPEG format. A serial flash memory is mounted for initialization of the image sensor [20]. The size of the camera controller board is 7x55 mm. A ~70-cm long multi-strand cable connects the camera head and the camera controller. The output of the camera controller connects to the wireless handle via a ~10-cm long USB 2.0 cable, although the camera controller can be readily integrated within the wireless handle if necessary.

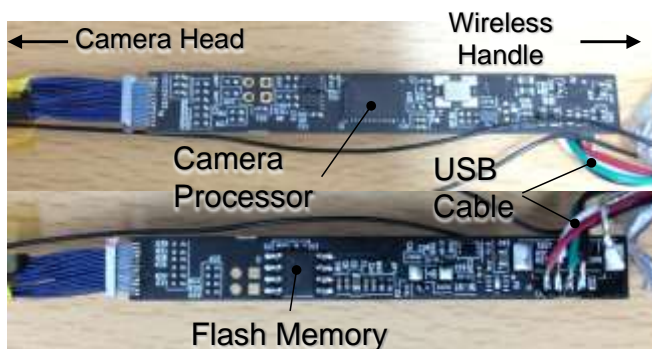


Fig. 5. Top and bottom side of the camera controller for the wireless endoscope.

C. Wireless Handle

Fig. 6 shows the configuration of the wireless handle. It transmits video data from the camera controller wirelessly using the UWB or the Wi-Fi link. The UWB or the Wi-Fi unit is exclusively powered (selected) through the mode switch. The USB cable from the camera controller connects to the input of the USB diplexer that delivers the video signal to either the UWB or the Wi-Fi unit depending on the position of the mode switch. The regulator converts the 5 V from the booster/charger to 3.3 V to supply the USB diplexer and the level shifter, and is implemented using an LDO (Low Dropout) regulator featuring low noise and low power characteristics [30]. Since the maximum output voltage of the mode switch (5 V) exceeds the maximum input control voltage level of the USB diplexer (3.3 V), a level shifter is employed to make the voltage levels compatible and is implemented using a Schmitt-trigger inverter [31]. The level shifter is powered by the 3.3 V generated by the regulator. The booster/charger converts the output voltage of the battery and charges it from an external source.

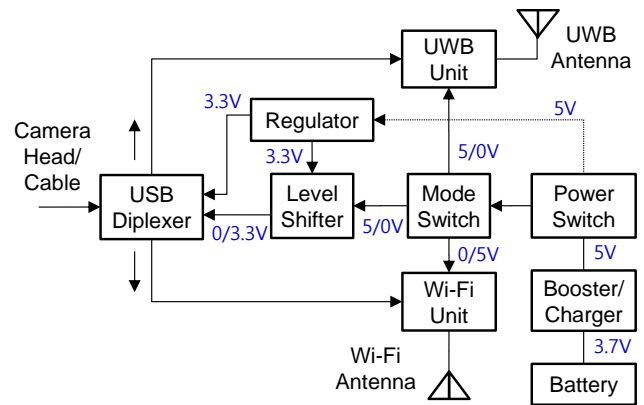


Fig. 6. Configuration of the wireless handle.

UWB is a communications technology with a wide bandwidth (typically defined as greater than 20% of the centre frequency or 500 MHz) [21]. It is typically characterized by high-speed, ultra-low power, and short range. UWB radios operate with very low transmit power and do not cause interference with electronic devices or other types of radios.

A commercial WUSB (Wireless USB) adaptor module implements the high-speed UWB unit [22], [23]. The UWB unit includes a broadband biconical antenna, widely adopted in UWB applications [24]-[26]. The size of the unit is 17x34x4 mm. There is a report of a wireless camera using the UWB unit [27]. The camera transmits videos with a resolution of 2048x1536 pixels (QXGA) at a frame rate of 15 fps in an MJPEG (Motion JPEG) format [27]. The maximum data transfer rate reached was ~40 Mbps. Therefore, this wireless handle should be able to support a camera head with a resolution higher than 1280x720 pixels.

A Wi-Fi UVC video router is employed for the Wi-Fi unit [28]. It is compliant with the IEEE 802.11 b/g/n standards. The unit works as an AP (Access Point) and any mobile device can directly connect to it without going through a Wi-Fi network. The size of the module is 35x25x18 mm, and this includes the PIFA (Planar Inverted-F Antenna) at the edge of the unit.

The USB signal from the camera controller connects to the UWB or the Wi-Fi unit depending on the selected communication mode. A high-bandwidth electronic USB diplexer handles the switching. It has a maximum on resistance of 10 Ω with a variation of 0.35 Ω [29]. It is powered by 3.3 V from a regulator, as its supply voltage range (3.0-4.3 V) is lower than 5 V.

The regulator converts the 5 V from the booster/charger to 3.3 V to power the USB diplexer and the level shifter, and is implemented using an LDO (Low Dropout) regulator featuring low noise and low power characteristics [30].

Since the maximum output voltage of the mode switch (5 V) exceeds the maximum input control voltage level of the USB diplexer (3.3 V), a level shifter is employed to make the voltage levels compatible and is implemented using a Schmitt-trigger inverter [31]. The level shifter is powered by the 3.3 V generated by the regulator.

The mode switch, connected to the power switch, selectively powers the UWB or the Wi-Fi unit. It also provides the control signal for the USB diplexer through the level shifter. The switch is a mechanical toggle unit with a DPDT (Double Pole Double Throw) configuration.

The power switch is a mechanical toggle unit with an SPDT (Single Pole Double Throw) configuration and is placed between the booster/charger and the mode switch to control the supply power to the wireless endoscope.

Over time, a slight degradation in the data transfer rate was observed caused by the heat from the communication units. A heat sink (an aluminium cooling fin and a ceramic plate) is mounted on each unit to mitigate the temperature rise, and is shown in Fig. 7. The battery is a cylindrical lithium-ion type generating 3.7 V, and a capacity of 2600 mAh [32].

The booster/charger steps up the battery output voltage of 3.7 V to 5.0 V to supply the UWB/Wi-Fi module, the regulator, the camera controller, and the camera head. The unit also charges the battery from an external 5 V source. All components are mounted on a two-layer FR-4 PCB with a size of 140x40 mm. The top and the bottom sides of the wireless handle are shown in Fig. 7.

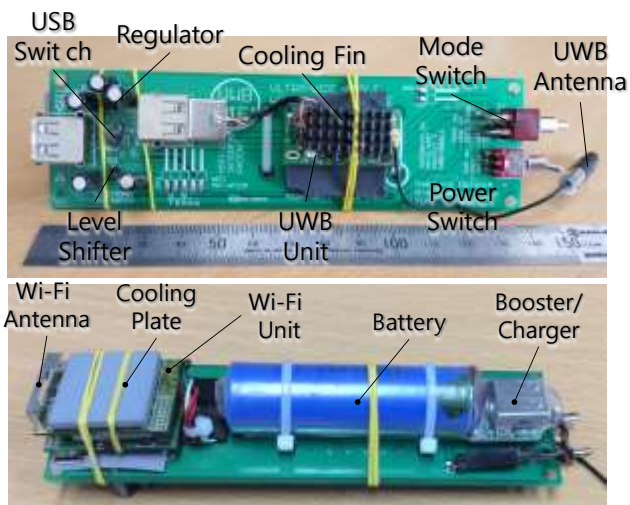


Fig. 7. Top and bottom side of the wireless handle.

IV. MEASUREMENT RESULTS

A. Field of View

The FOV measurement on the proposed endoscope is compared with that on a commercial unit (WF200) [11]. Two camera heads are attached and positioned at the same height above a grid pad (Fig. 8). The vertical distance between the camera heads and the pad is 38 mm. The size of a square cell in the pad is 10x10 mm. The transmitted video from the proposed and the commercial unit is displayed via a laptop and a mobile tablet, respectively [33]. The horizontal and the vertical FOV of the proposed endoscope is estimated to be 69° and 117° , respectively, with the diagonal FOV as 130° (Fig. 9). Moderate barrel distortion is observed due to the ultra-wide-angle characteristic of the lens module. To the best of the author's knowledge, the proposed endoscope has the largest FOV among all existing wireless endoscopes. The measured FOV is smaller than the AOV of the lens module (150°) since the image sensor can cover only a part of an incident image through the lens module. The horizontal, the vertical, and the diagonal FOV of the commercial unit are estimated to be 46° , 33° , and 55° , respectively (Fig. 10). The FOV of the proposed endoscope is more than twice that of the commercial unit.



Fig. 8. FOV measurement setup.

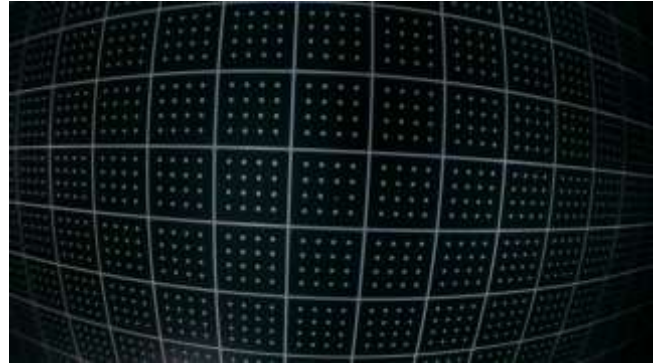


Fig. 9. Grid photo by the proposed ultra-wide-angle endoscope.

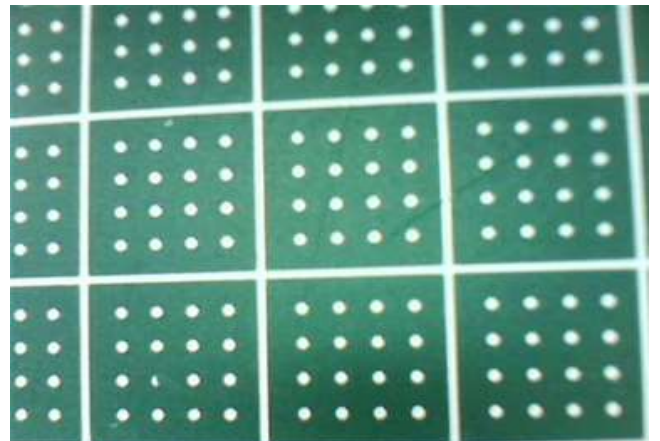


Fig. 10. Grid photo by the commercial wireless endoscope (WF200) [11].

B. Video Performance

The video performance of the wireless endoscope is evaluated along with the resolution, the frame rate, and the data transfer rate. The wireless handle and a receiver (UWB or Wi-Fi adaptor) are placed within LOS (Line-of-Sight) at a distance of 2 m. A free and open source cross-platform multimedia player and a framework (VLC) are used to measure the video performance [34]. The endoscope operates at 720p HD resolution (1280x720 pixels) at a frame rate of 30 fps in the UWB mode. The maximum data transfer rate reaches ~ 37 Mbps. The endoscope operates in the Wi-Fi mode at the same resolution, but has a much lower data transfer rate (~ 8 Mbps Max.). Although VLC does not provide a frame rate in the Wi-Fi mode, after comparing the measured data transfer rates, it is estimated to be more than four times lower than the frame rate of the UWB mode.

C. Latency

The video latency of the UWB link is measured using the setup shown in Fig. 11 [27]. The camera head is positioned to observe a running stopwatch. Its video output is transmitted to the host UWB adapter plugged into a laptop and is displayed on the screen. The video latency can be estimated from the time difference of the original and the captured stopwatch window. The camera has a latency of ~0.1 sec for the UWB mode. To measure the latency in the Wi-Fi mode, an embedded adaptor in the laptop is connected to the Wi-Fi unit in the wireless handle. Following the same method, the Wi-Fi unit shows a latency of ~0.5 sec (Fig. 12). The larger latency in the Wi-Fi mode of operation can be explained mainly by the lower data transfer rate and the lower frame rate. The overall power consumption of the endoscope is measured to be 1.5 and 2.1 W at the UWB and the Wi-Fi operation modes, respectively. The performances of various commercial endoscopes are compared in Table I.



Fig. 11. Latency measurement in UWB communication mode.



Fig. 12. Latency measurement in Wi-Fi communication mode

V. CONCLUSION

An ultra-wide-angle wireless endoscope was demonstrated with an FOV of 130° and with HD resolution (1280x720 pixels). The lens module is implemented with all-plastic lenses to have an AOV of 150°. The lenses are manufactured by a plastic injection-molding process to reduce the cost. The endoscope employs a BCC architecture to physically separate the camera controller from the camera head. The compact structure of the camera head is achieved using a serial CMOS image sensor with a MIPI CSI-2 interface. The horizontal and the vertical FOV of the proposed endoscope are estimated to be 69° and 117°, respectively, with the diagonal FOV as 130°.

TABLE I
SUMMARY OF PERFORMANCE COMPARISON

Ref.	FoV (deg.)	Resolution (pixels)	Frame Rate (fps)	Dia. (mm)	Communication
[7]	60	640x480	30	9	WiFi
[8]	NA	640x480	NA	9.8	WiFi
[9]	50	640x480	30	17	WiFi
[10]	105	1.3M	NA	NA	5.8 GHz
[11]	60	1280x720	NA	8.5	WiFi
This work	150	1280x720	30/ NA	11.2 (8x8)	UWB/ WiFi

The wireless handle includes the UWB and the Wi-Fi communication units for the wireless video transmission. The UWB link supports a maximum data transfer rate of ~37 Mbps to transmit videos with a resolution of 1280x720 pixels and a frame rate of 30 fps in the MJPEG format. The endoscope also supports the Wi-Fi operation mode for enhancing the interoperability with various mobile devices, although at a relatively lower speed (~8 Mbps Max.). The latency of the endoscope is measure to be ~0.1 sec in the UWB mode. A noticeable latency (~0.5 sec) is observed in the Wi-Fi mode due to its lower data transfer rate.

These results suggest that the proposed BCC architecture along with the high-speed UWB link should be able to keep pushing the resolution of a wireless endoscope above HD-levels while keeping the size of the camera head and the cable compact. The proposed endoscopy structure will open up the path to a higher-performance yet low-cost wireless endoscopy.

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